

Because of the net free charge in the diffuse layer, if you apply a tangential electric field you get motion! This is called electroosmosis and is very useful in μ fluidic systems.

First, what is the free charge density $\delta^{(f)}$? Recall that we had

the Boltzmann distribution:

$$n^k = n_b e^{-\frac{eZkT}{kT}}$$

we defined $\Psi = \frac{eZkT}{kT} - \Psi(\frac{ZkT}{Z})$ +1 or -1
dep. on + or -
charge

$$\text{so } n^k = n_b e^{-\Psi(\frac{ZkT}{Z})}$$

That's because, say, positive ions are attracted to a negative surface & neg. ions are repelled!

Suppose we have a $Z-Z$ electrolyte where the bulk concentration of each is n_b

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(They have to be the same for electro-
neutrality). The net free charge is:

$$g^{(f)} = e \sum n^k z^k = e n_b z \left(e^{-\bar{\Psi}} - e^{\bar{\Psi}} \right)$$

For 1-1 electrolytes, $z=1$

We also had, for some surface potential $\bar{\Psi}_s$:

$$\bar{\Psi} = 2 \ln \left(\frac{1 + e^{-Kx} \tanh(\frac{1}{4}\bar{\Psi}_s)}{1 - e^{-Kx} \tanh(\frac{1}{4}\bar{\Psi}_s)} \right)$$

$$\text{so } e^{-\bar{\Psi}} = \left(\frac{1 - e^{-Kx} \tanh(\frac{1}{4}\bar{\Psi}_s)}{1 + e^{-Kx} \tanh(\frac{1}{4}\bar{\Psi}_s)} \right)^2$$

and $e^{\bar{\Psi}}$ is just the inverse.

It is convenient (but not necessary!) to work w/ the low $\bar{\Psi}_s$ limit:

$$\bar{\Psi} \approx \bar{\Psi}_s e^{-Kx}$$

$$\text{and so } g^{(f)} = -2e n_b z \sinh(\bar{\Psi})$$

$$x = -2e n_b z \bar{\Psi}_s e^{-Kx}$$

If we recall that $\kappa^{-1} = \left(\frac{\epsilon \epsilon_0 kT}{2e^2 z^2 n_b} \right)^{1/2}$ 386

we can recast this as:

$$\varphi^{(f)} \approx -\epsilon \epsilon_0 \kappa^2 \psi_s e^{-\kappa x}$$

or, as usually written,

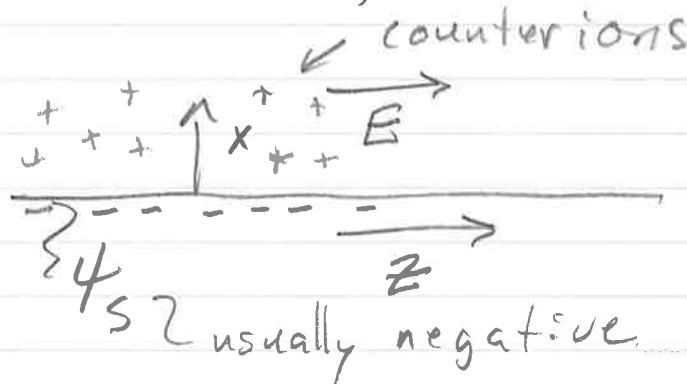
$$\varphi^{(f)} = -\epsilon \epsilon_0 \kappa^2 \zeta e^{-\kappa x}$$

↳ known as the zeta potential

The ζ zeta potential is known as the potential at the shearing surface, but for small ζ it is just ψ_s - for large potentials there is a "bound" Stern layer of counter-ions that have low mobility.

Ok, now we apply a tangential field

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There is a force per volume on the fluid :

$$\sigma = \mu \frac{\partial^2 u_z}{\partial x^2} + \sigma^{(f)} E$$

$$\text{so : } \frac{\partial^2 u_z}{\partial x^2} = - \frac{\sigma^{(f)} E}{\mu} = \frac{\epsilon \epsilon_0 K^2 \xi}{\mu} e^{-Kx} E$$

Let's scale :

$$x^* = Kx \quad u_z^* = \frac{u_z}{U_c}$$

~~$$\therefore K^2 U_c \frac{\partial^2 u_z^*}{\partial x^{*2}} = E \frac{\epsilon \epsilon_0 K^2 \xi}{\mu} e^{-x^*}$$~~

$$\therefore U_c = \left(\frac{\epsilon \epsilon_0 \xi}{\mu} \right) E$$

$$\text{and } \frac{\partial^2 u_z^*}{\partial x^{*2}} = e^{-x^*}$$

Integrating once :

$$\frac{\partial u_z^*}{\partial x^*} = -e^{-x^*} + C_1$$

At infinity the stress is zero, so $C_1 = 0$

Integrating again:

$$u_z^* = e^{-x^*} + C_2$$

$$\text{but } u_z^*|_{x^*=0} = 0 \quad (\text{no-slip}) \therefore C_2 = -1$$

$$\text{so } u_z^* = e^{-x^*} - 1$$

Far away (but remember how short K^{-1} is!)

$$u_z^* = -1$$

So our electroosmotic velocity is just $-U_0$!

The quantity $\frac{\epsilon\epsilon_0\zeta}{\mu}$ is the electroosmotic mobility. Note that this is independent of n_b ! It only depends on ζ and fluid properties!

Why? If n_b increases, so does $\zeta^{(f)}$ but since K^{-1} decreases viscous drag (which goes as K^2) cancels this out!

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So what is $\mu_{eo} = \frac{\epsilon \epsilon_0 \xi}{\mu}$ = electroosmotic mobility?

We can plug in some numbers!

Say $\xi = 100 \text{ mV}$ (typical value)

$\mu = 10^{-3} \text{ Pas}$ (or 1 cP) and $\epsilon = 80$ (water)

This yields:

$$\mu_{eo} = 7.08 \times 10^{-8} \frac{\text{m/s}}{\text{V/m}}$$

The more usual units are:

$$\mu_{eo} = 7.08 \frac{\text{mm/s}}{\text{V/cm}}$$

as microfluidic channels are pretty short!

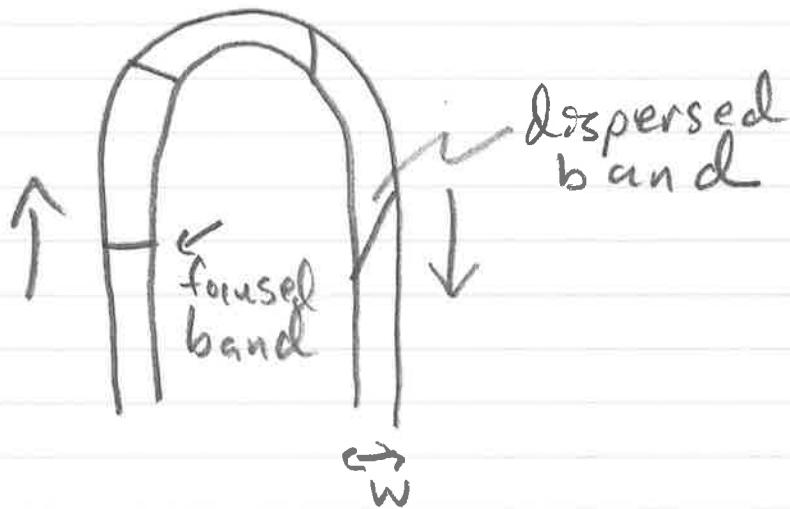
This is a good approx provided ξ isn't too big. For larger values, just integrate the exact solution numerically!

EO velocities are small, but they are very useful for driving fluid through thin channels! For pressure driven flow

The velocity goes as depth². That means that for, say, $50\mu\text{m}$ deep channels you need a large ΔP ! For EO the velocity is order of depth.

Another advantage - there's no shear as you get plug flow - essentially slip at the walls! For a straight channel there's no dispersion!

Now for disadvantage: For a large aspect ratio channel curves are huge sources of dispersion due to the "race track effect":



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The explanation is simple: The inside of the 180° bend is πW shorter than the outside. This means a higher electric field and a shorter distance. A focused band smears out by $2\pi W$ after every bend, which really adds up on a serpentine channel (needed for length). Modifications to the width profile can reduce this, but it's still a problem!

Another issue is the generation of the electric field. To get any field beyond K^{-1} thickness (really short) you have to have a current! That means an electrode reaction at each end! This is usually producing electrolysis, acid & base (pH change) and bubbles -

all of which cause trouble!

A last disadvantage: If you have a slug of mixed solutes, the electric field will separate them. This can be undesirable, but is actually the basis of capillary electrophoresis, our next topic!

Suppose we have a particle of radius a and surface charge Q . If $Ka \ll 1$ (e.g. really small particle or a low n_0) then the diffuse layer is spread out! If we apply an electric field E_∞ then the force is just $E_\infty Q$. This is balanced by Stokes Law drag:

$$E_\infty Q = 6\pi\mu La u$$

The electrophoretic mobility of the particle is :

$$\mu_{\text{ep}} = \frac{Q}{6\pi\mu a} ; u = \mu_{\text{ep}} E_{\infty}$$

For a thin double layer $Ka \gg 1$ and we have a more complicated result. Essentially, you get EO flow at the surface of the particle (in the double layer) and the particle moves in the opposite direction of this!

We get :

$$u = \frac{Q}{4\pi\mu a} \frac{1}{Ka} E_{\infty}$$

or, in terms of the ξ potential :

$$u = \frac{\epsilon \epsilon_0 \xi}{\mu} E_{\infty}$$

which is indep of a as $\frac{Q}{4\pi a^2}$ is the charge density

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Because of this, mobilities in an electric field are used to measure the potential of colloids.

So how is this used in capillary electrophoresis? A mixture of analytes (pos or neg charge!) are drawn through the capillary by electroosmosis: The EO velocity needs to be higher than the neg. vel of opposite charge species.

Species w/ different charge or size move w/ dif. velocities and separate into bands for detection at the end of the capillary.

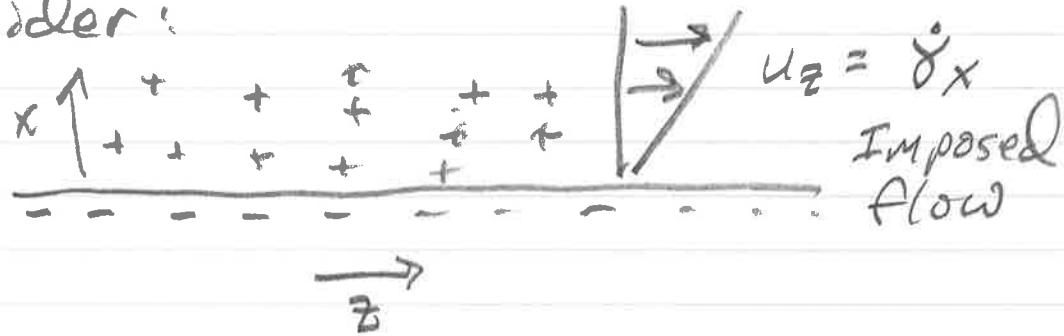
A key is initial focusing of the band at injection using stacking: If you suspend the analyte in a low conc. buffer at the entrance it will focus at the

lead edge due to a higher electric field in the initial slug (low conductivity = high field for same current).

Other tricks are things like iso-electric focusing: The charge on a protein depends on the pH. If you put it in an axial pH gradient it will focus at its isoelectric point (pH of neutral charge) and be convected along w/ the EO velocity. Many other variations have also been developed!

Another way the diffuse layer, EO and electrophoresis can combine is if you also have a shear flow in the absence of an imposed electric field. This leads to a streaming potential.

Consider:



If there's no electric field the positive counter ions are swept along with the shear flow. This net current will (like a Van de Graaf generator) lead to a charge buildup! The current

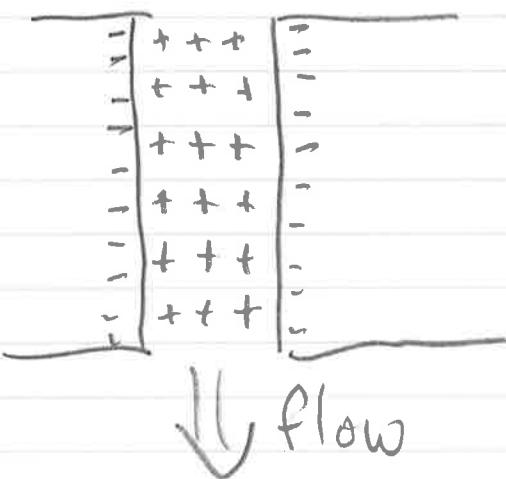
scales as $(K^{-1}\delta) K^{-1} \cdot w \cdot g^{(f)}$

$\underbrace{K^{-1}\delta}_{\substack{\text{char. vel.} \\ \text{velocity}}}$
 $\underbrace{w}_{\substack{\text{length} \\ \text{in to paper}}}$
 $\underbrace{g^{(f)}}_{\substack{\text{avg. free charge} \\ \text{extension}}}$

Since it goes as $(K^{-1})^2$ it is most important for large K^{-1} (low ion conc. in the bulk) and is quite a problem in pumping gasoline! Ground your pipes to avoid sparks!

This is also important for charged pores in membranes.

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If the pore radius is comparable to k_f^{-1} pressure driven flow leads to a net convection of counter ions across the membrane. By overall electro neutrality this leads to a membrane polarization and EO flow back the other way!

Polarization can also occur if a membrane is permeable to some ions but not others - Diffusion alone can lead to a Donnan potential - which is how your nerves work! Electrophysics is a huge subject! This is just an introduction!